



Monitoring hemodynamic parameters in heart failure patients with wearable RF sensing

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Declaration of conflict of interest related to the topic

Minority share holder of PrecorDx b.v.

Stuck at home during Covid-19

Bart Steensma



MRI : RF coil/antennas are motion sensors


- Reflection & scattering of RF fields is modulated by the motion of tissue structures
- This can be measured either actively by monitoring antenna impedance over time or passively by thermal noise modulations.

Buikman D, Helzel T, Roschmann P. The RF coil as a sensitive motion detector for magnetic resonance imaging. Magn Reson Imaging 1988;6:281–289.

IMAGING METHODOLOGY - Notes

Magnetic Resonance in Medicine 80:633–640 (2018)

Cardiac Gating Using Scattering of an 8-Channel Parallel Transmit Coil at 7T

Sven H.F. Jaeschke , Matthew D. Robson, and Aaron T. Hess *

Purpose: To establish a cardiac signal from scattering matrix or scattering coefficient measurements made on a 7T 8-channel parallel transmit (pTx) system, and to evaluate its use for cardiac gating.


Methods: Measurements of the scattering matrix and scattering coefficients were acquired using a monitoring pulse sequence and

Key words: parallel transmit; cardiac gating; motion sensor; cardiac MRI; reflected power; RF scattering

COMPUTER PROCESSING AND MODELING - Notes

Magnetic Resonance in Medicine 79:1730–1735 (2018)

Respiratory Motion Model Based on the Noise Covariance Matrix of a Receive Array

A. Andreychenko *,^{1*} B. Denis de Senneville,^{1,2} R.J.M. Navest,¹ R.H.N. Tijssen,¹ J.J.W. Lagendijk,¹ and C.A.T. van den Berg¹

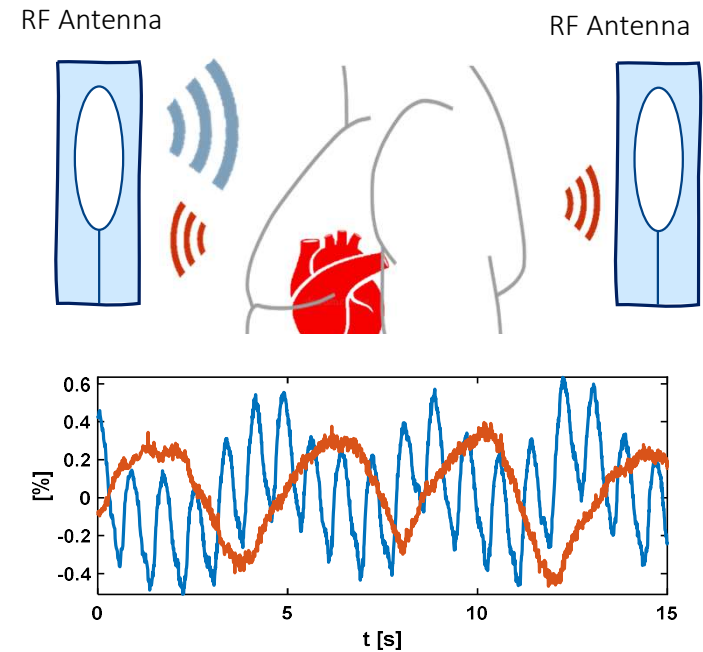
Purpose: Tracking of the internal anatomy by means of a motion model that uses the MR-derived motion fields and noise covariance matrix (NCM) dynamic as a surrogate signal.

Methods: A 2D respiratory motion model was developed based on

be directly quantified. However, the motion information obtained from such systems is strongly limited by the update time and latency constraints imposed by the MR-based tracking system. An alternative approach consists of

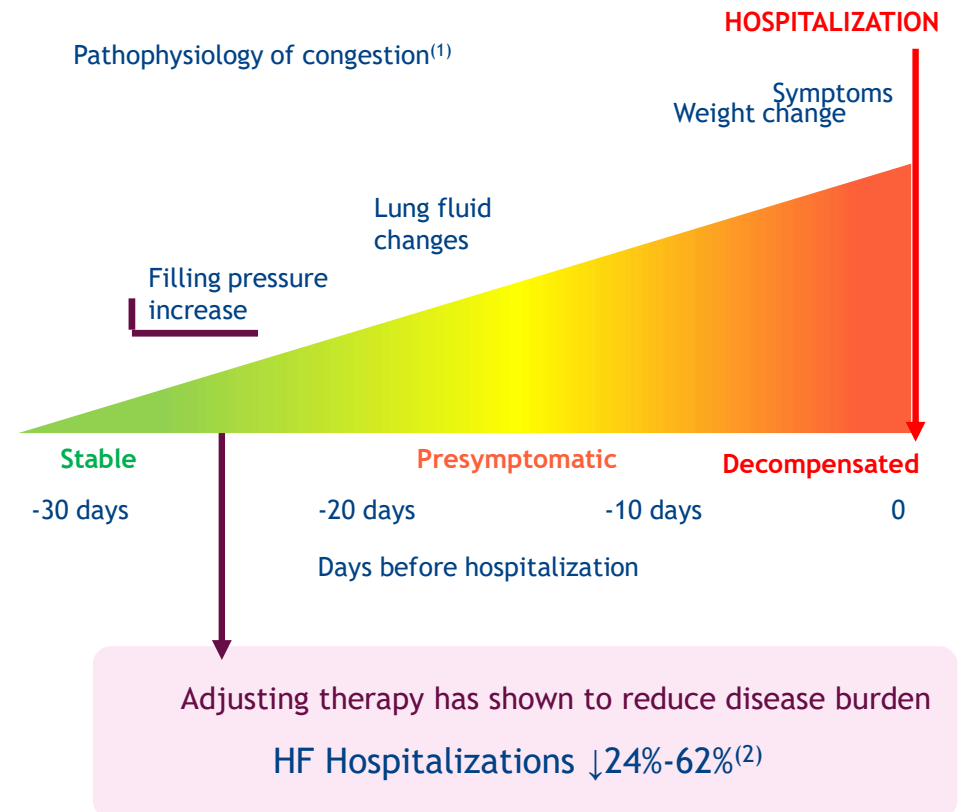
Radiofrequency Sensing of heart

- Actively monitoring impedance of RF antennas placed on body with a nano-VNA
- $Z_{11}(t)$ or $Z_{12}(t)$
- We could easily observe both imprint of respiration and cardiac induced motion
- These are caused by **mechanical** motion
- Can we use RF antennas to monitor pumping function of the heart in a **non-invasive manner**?



Chronic heart failure is a severe and growing healthcare problem

- 64M patients worldwide
- HF deteriorates from chronic to acute unnoticably
- Home monitoring of heart function -> medication optimization -> prevents hospitalization



Invasive sensors to monitor heart function for heart failure

- Most common methods such as ECG, or weight monitoring lack sensitivity to mechanical pumping function.

HeartLogic

CRT device based algorithmic HF monitoring

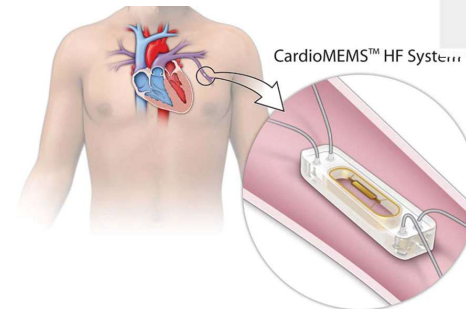
Boston Scientific
Advancing science for life™



CardioMEMS

Invasive PA monitoring

Abbott

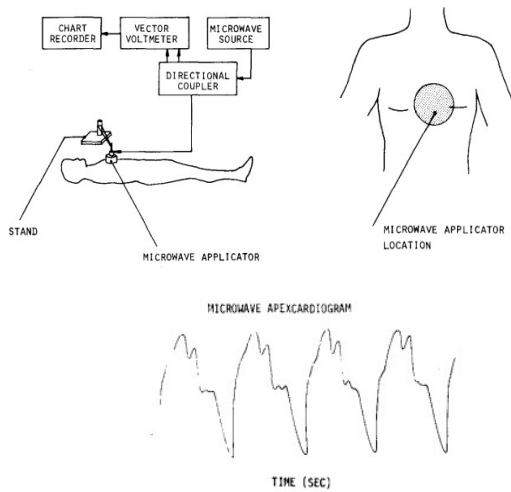


NATIONAL
MEDICARE RATE
\$29,460

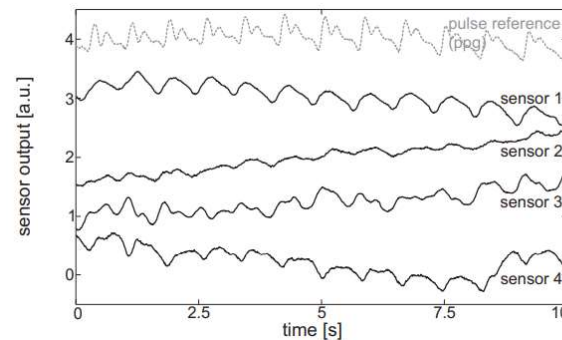
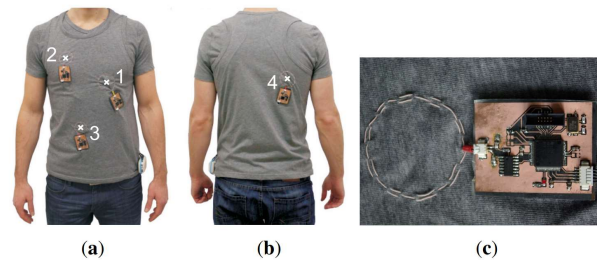
Invasive procedure required -> costs + potential complications

Can this be done in non-invasive manner by RF sensing?

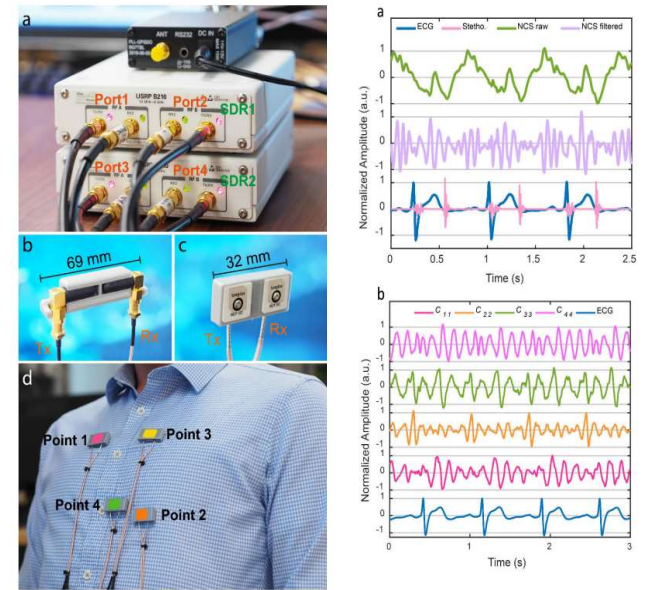
Large variety of RF sensing for cardiac motion exists outside MRI field



1. Microwave Apexcardiography
 Frequency range: 2100 – 2500 MHz
 Lin et al, 1979, IEEE TMTT, 27:6



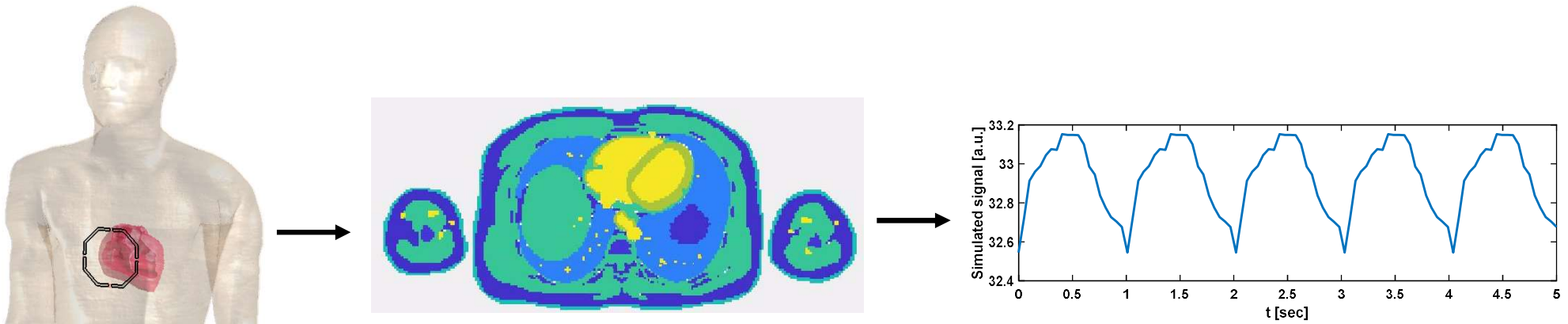
2. The MAIN Shirt: A Textile-Integrated Induction Sensor Array
 Frequency range: 17-20 MHz
 Teichmann et al, Sensors 2014, 14, 1039-1056



3. Near field coherent sensing
 Frequency range: 900-950 MHz
 Hui et al, Nature Electronics 2018, 1, 74-78

EM simulations provide a better understanding of RF sensing signal

- Sim4Life (Zurich Medtech, Zurich, Switzerland)
- 4D XCAT model with beating heart (Segars et al, Phys Med Biol 2010)
- Predict interaction RF coil with body



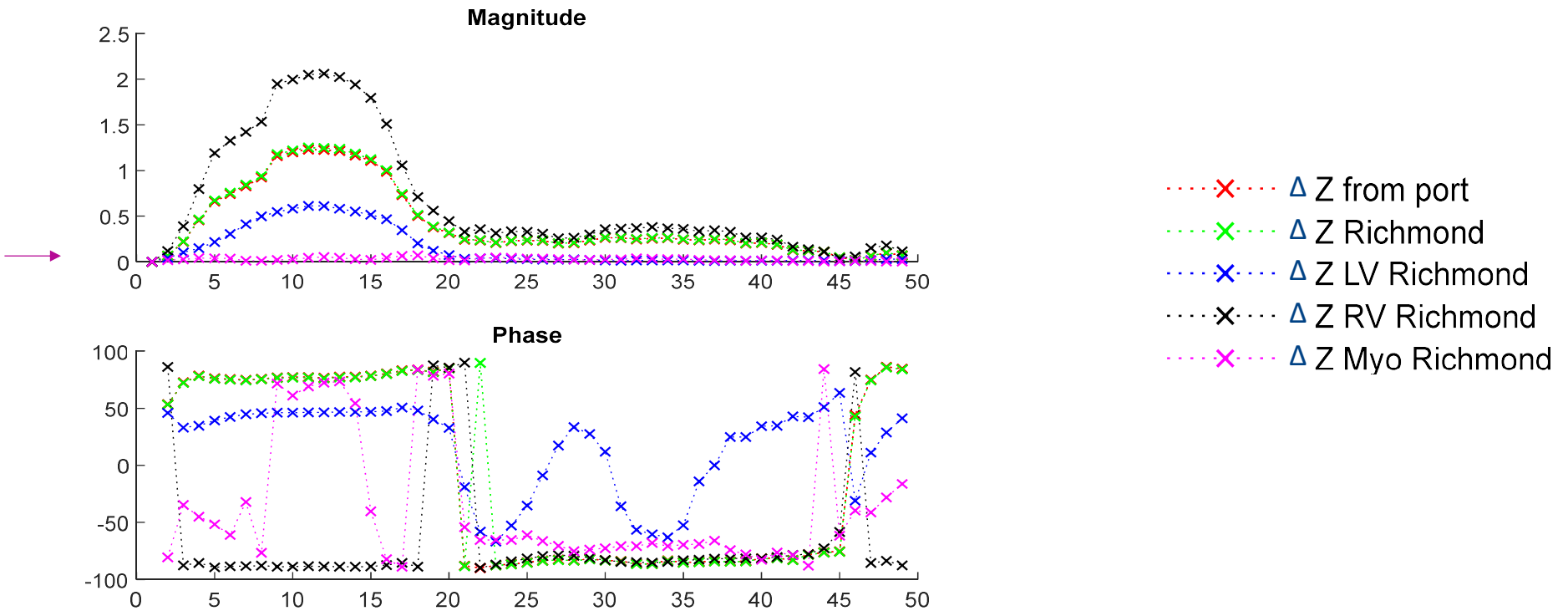
Spatial sensitivity of RFS to cardiac motion is described by Reaction theorem¹

$$\underbrace{Z_t - Z_0}_{\text{Signal}} = - \overbrace{\frac{j\omega}{I^2}}^{\text{freq}} \int_V \underbrace{(\epsilon_{r,t} - \epsilon_{r,0})}_{\text{Tissue params}} \underbrace{E_{r,t} \cdot E_{r,0}}_{\text{EM field}} dV$$

\int_V



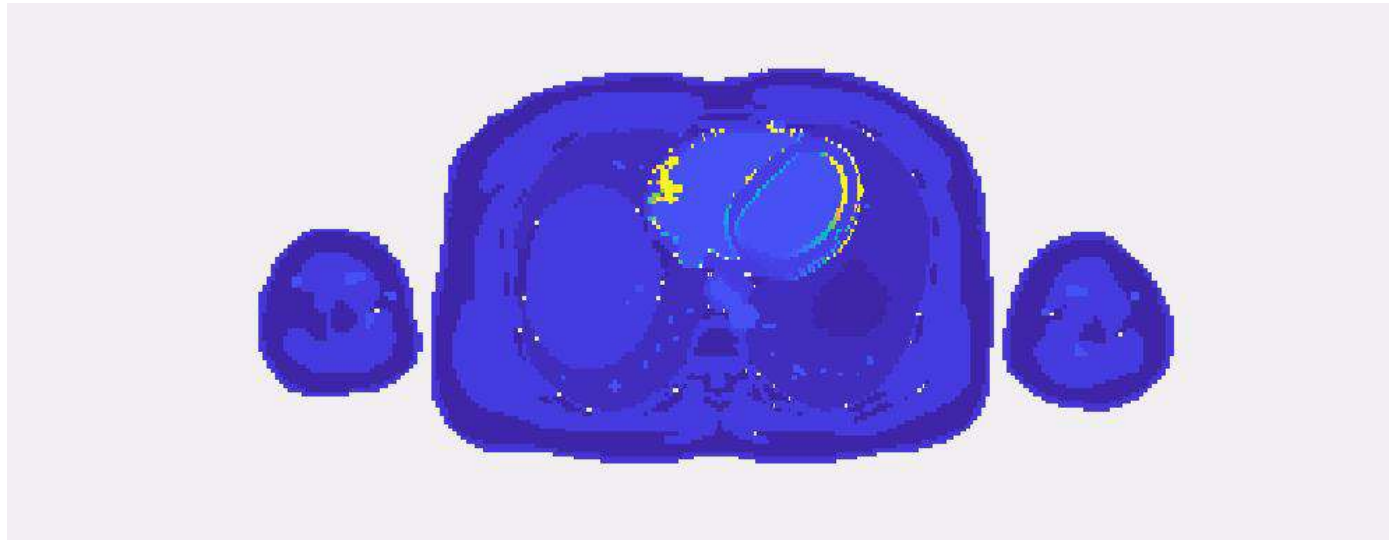
Verifying port's and field's perspectives on Z modulation

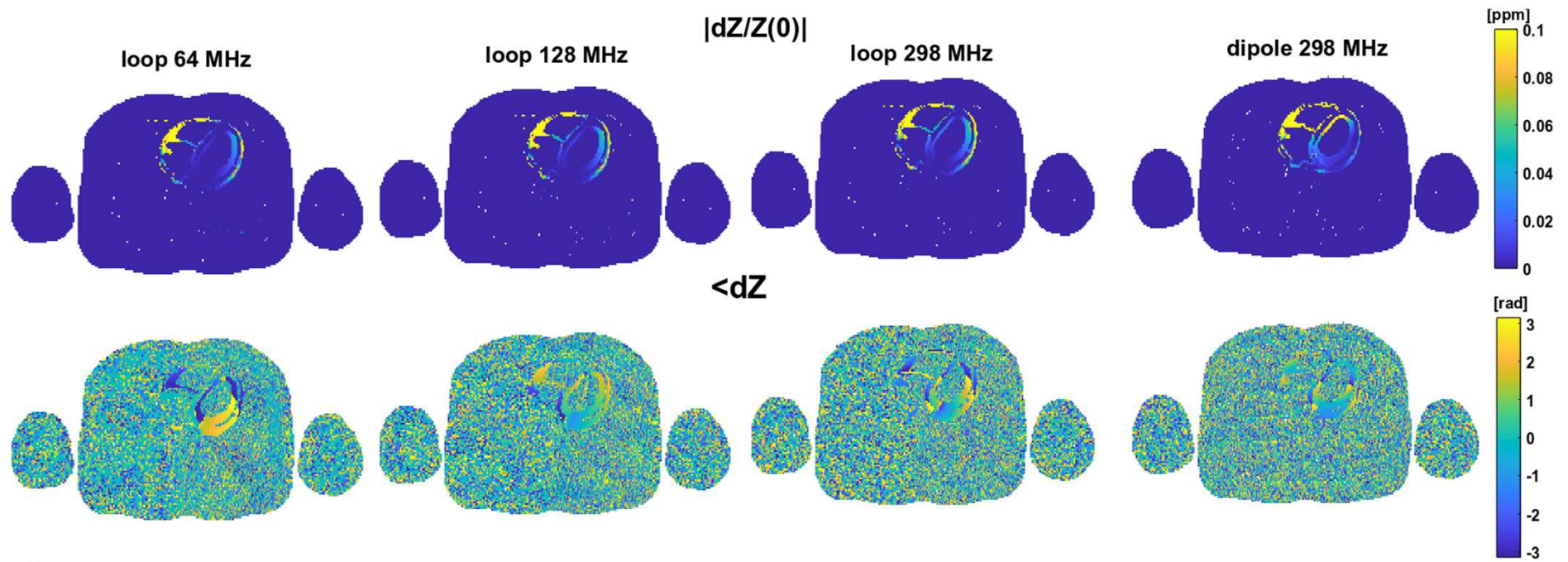


$$Z(t) - Z(0) = -\frac{i\omega}{I^2} \int_V [(\epsilon(r,t) - \epsilon(r,0)) E(r,t) \cdot E(r,0)] dV = \int_V dZ dV$$

Richmond. IRE transactions on antennas and propagation. 1961

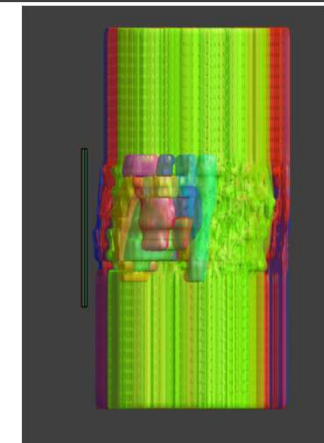
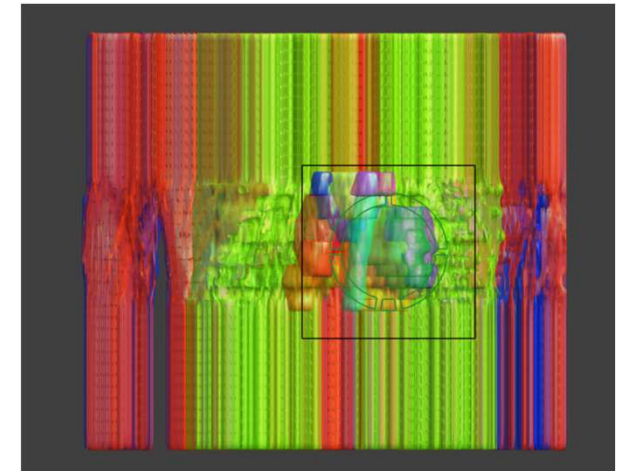
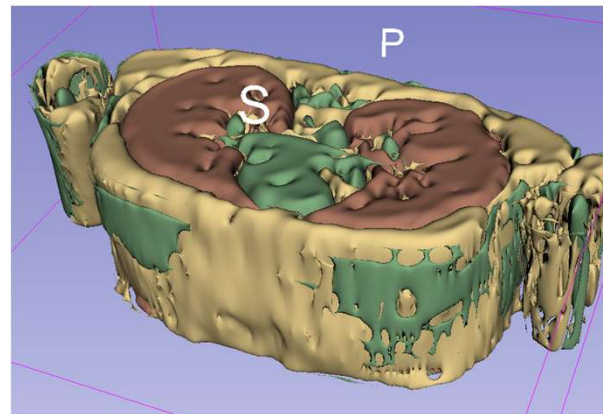
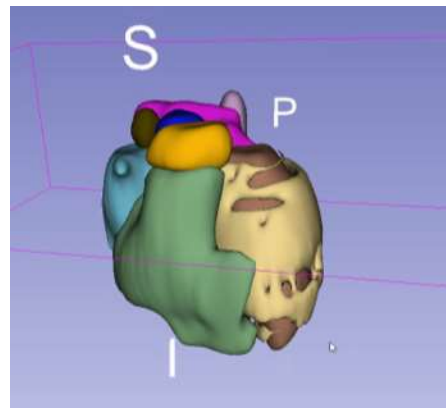
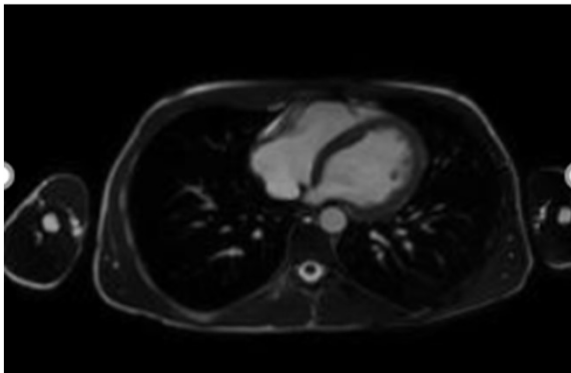
Loop antenna is sensitive to edges of heart moving through EM field



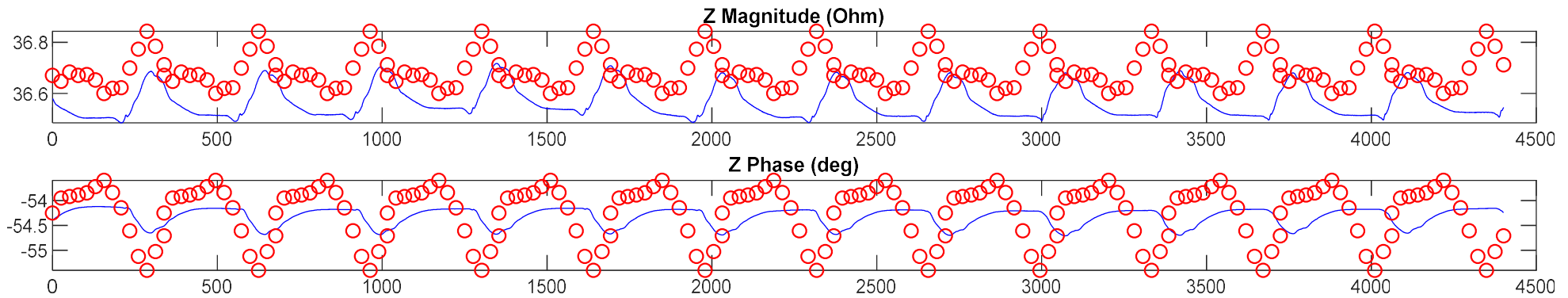


Validation with a subject specific model based on MRI

2d Transverse CINE
FOV 400*250*100 mm³
Res 1.8*1.8*10 mm³



Matching between simulation and measurement



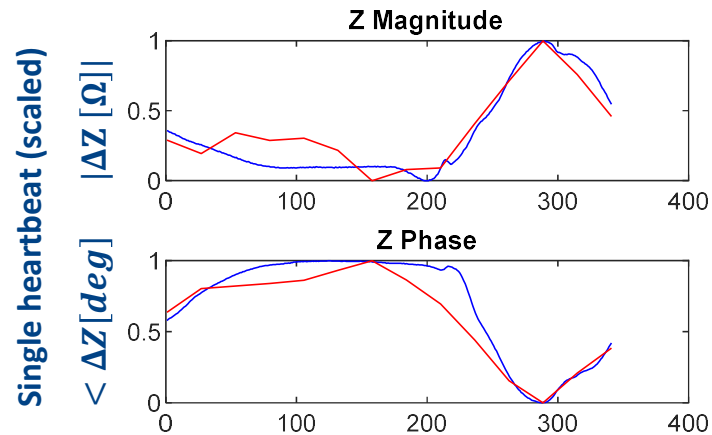
Time →



Christina Louka

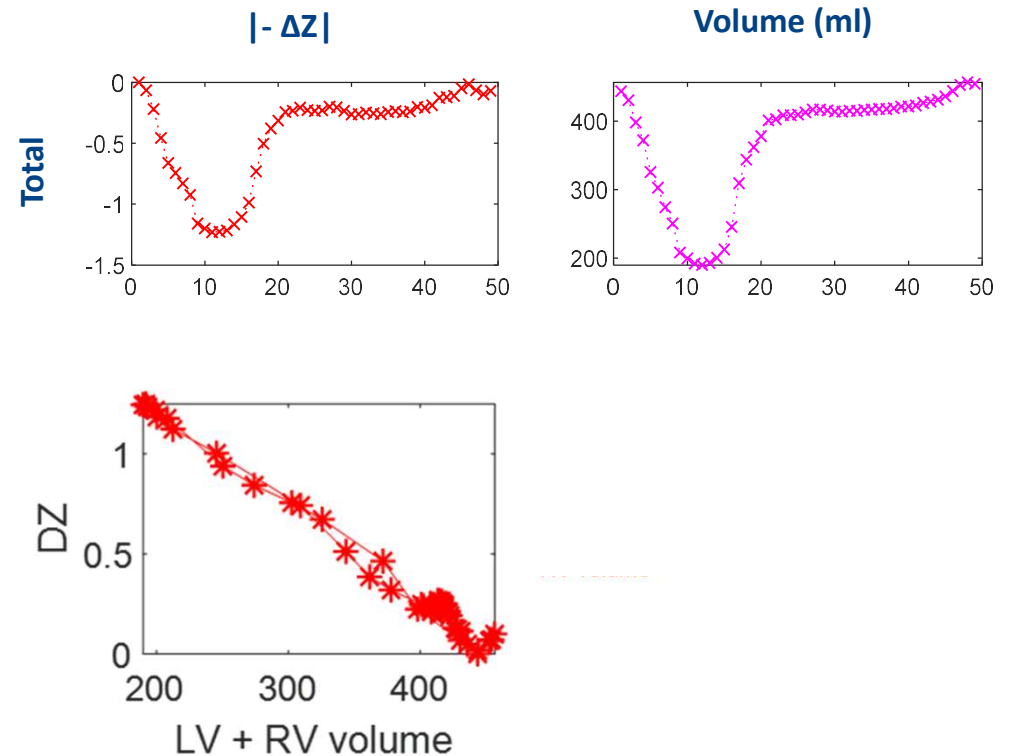
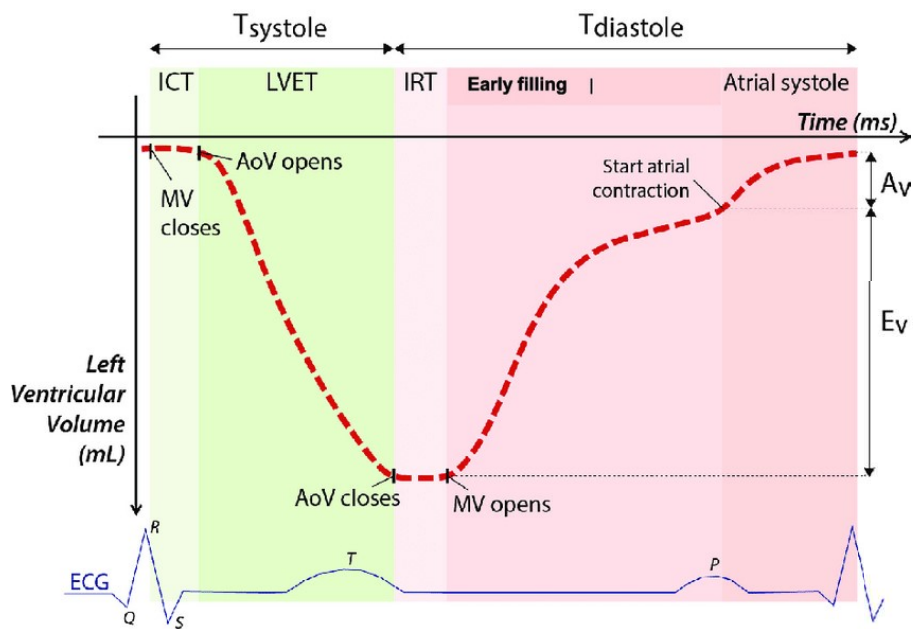


Flavio Meliado



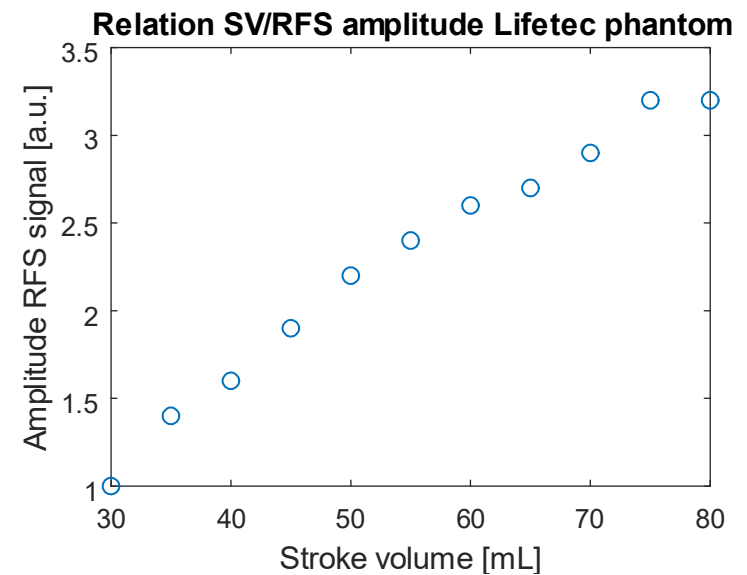
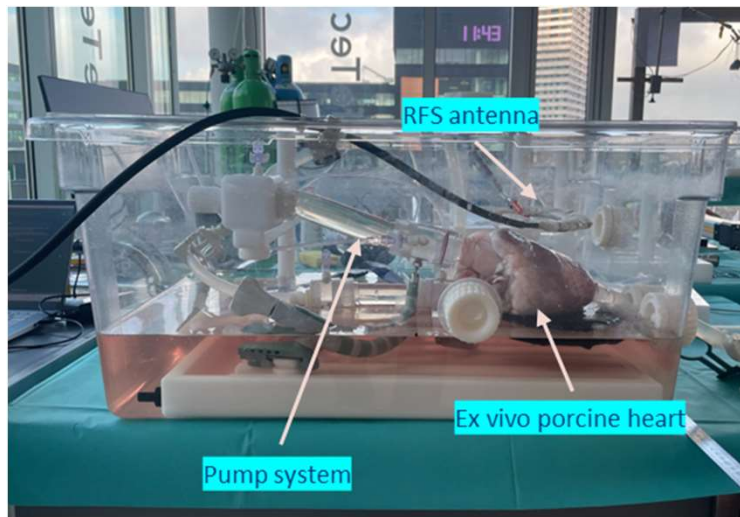
— measurement
— simulation

Near-linear relation between RFS signal and ventricular volumes



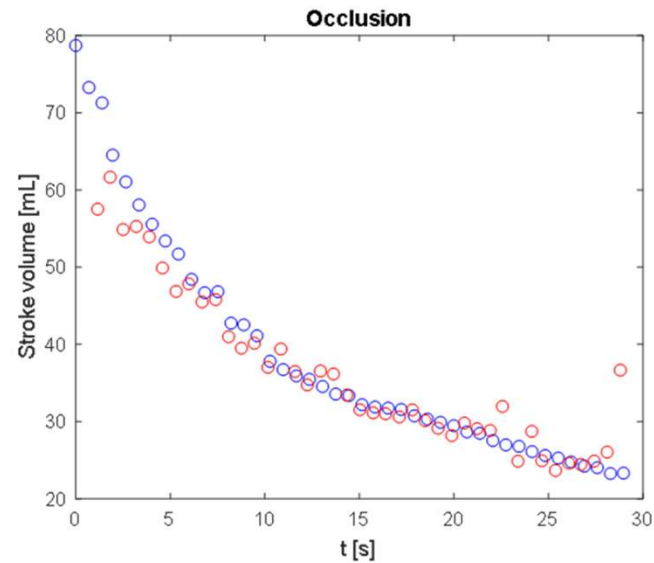
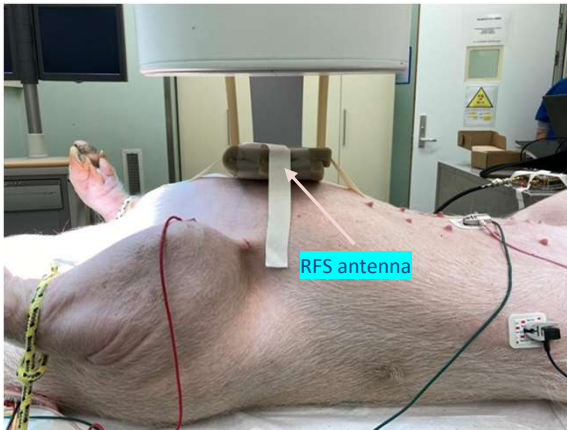
Ex vivo experiments in controlled environment confirm sensitivity to stroke volume

- The Lifetec Group, Eindhoven, The Netherlands
- Stroke volume gradually increased over time

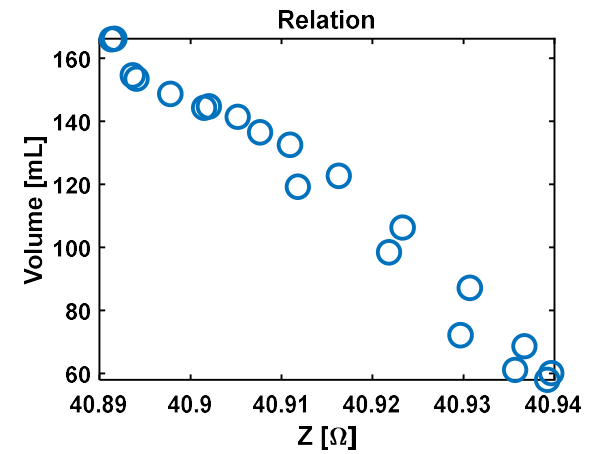
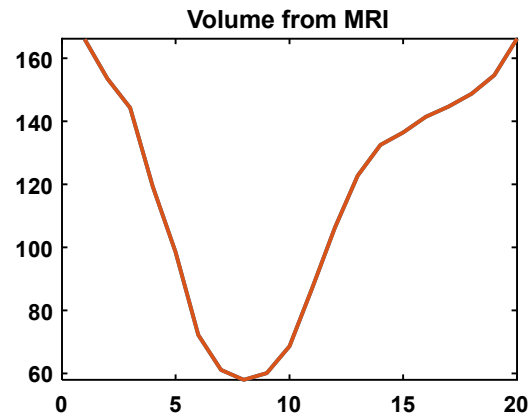
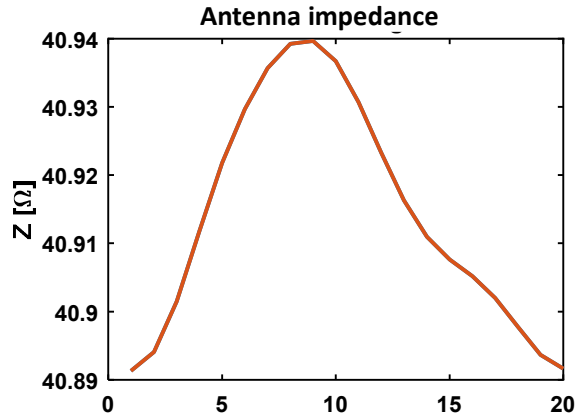
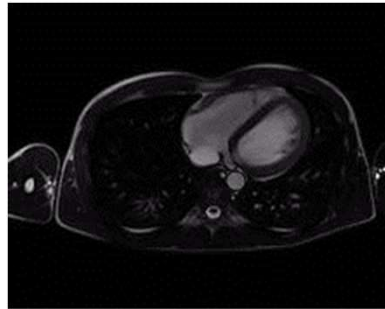


In vivo porcine stroke volume correlates to amplitude RFS

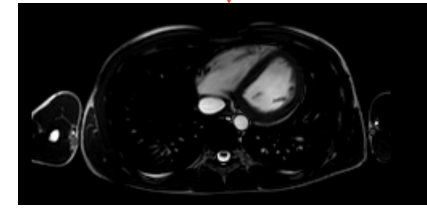
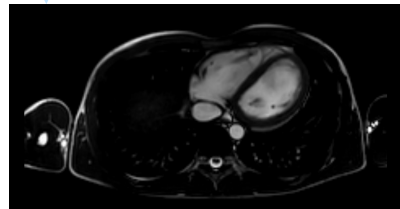
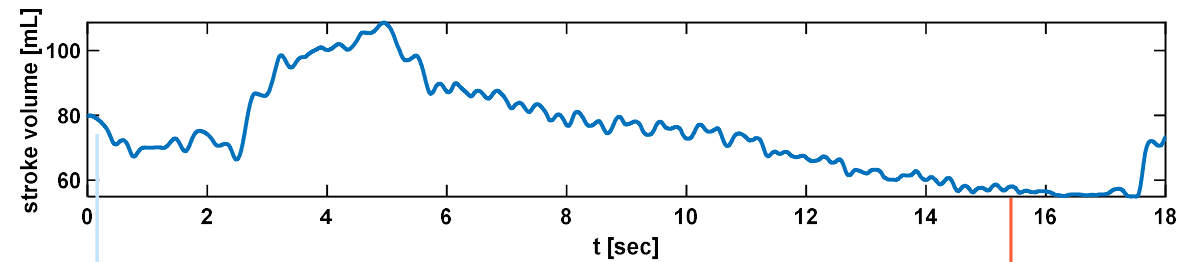
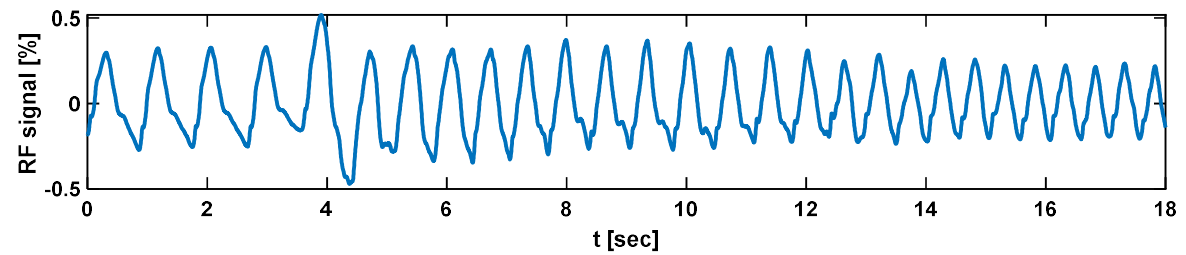
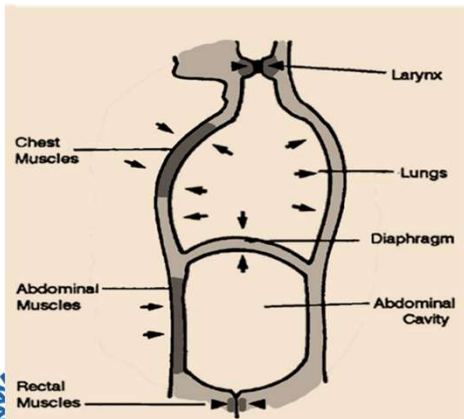
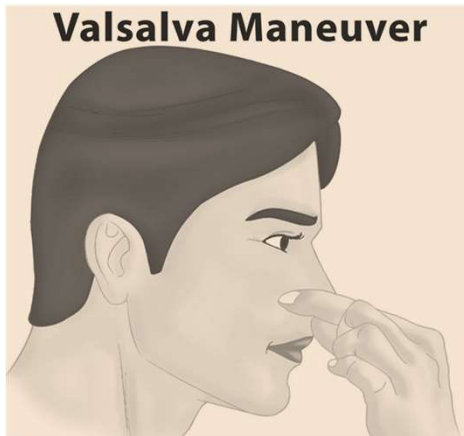
- Existing experiments were occlusion balloon is tested (cardiothoracic surgery)
- Stroke volume and pressure are measured with admittance catheter (van Hout et al, Physiol Rep 2014)



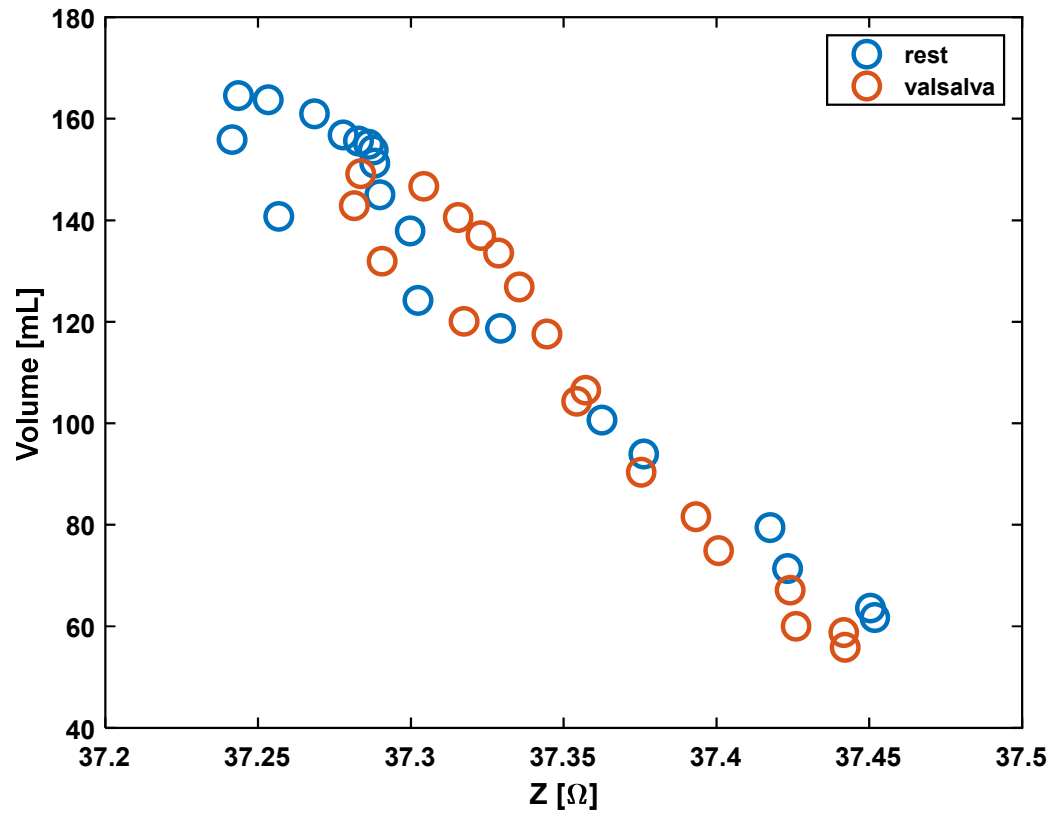
Experimental comparison to MRI shows linear relationship between RF signal and LV volume



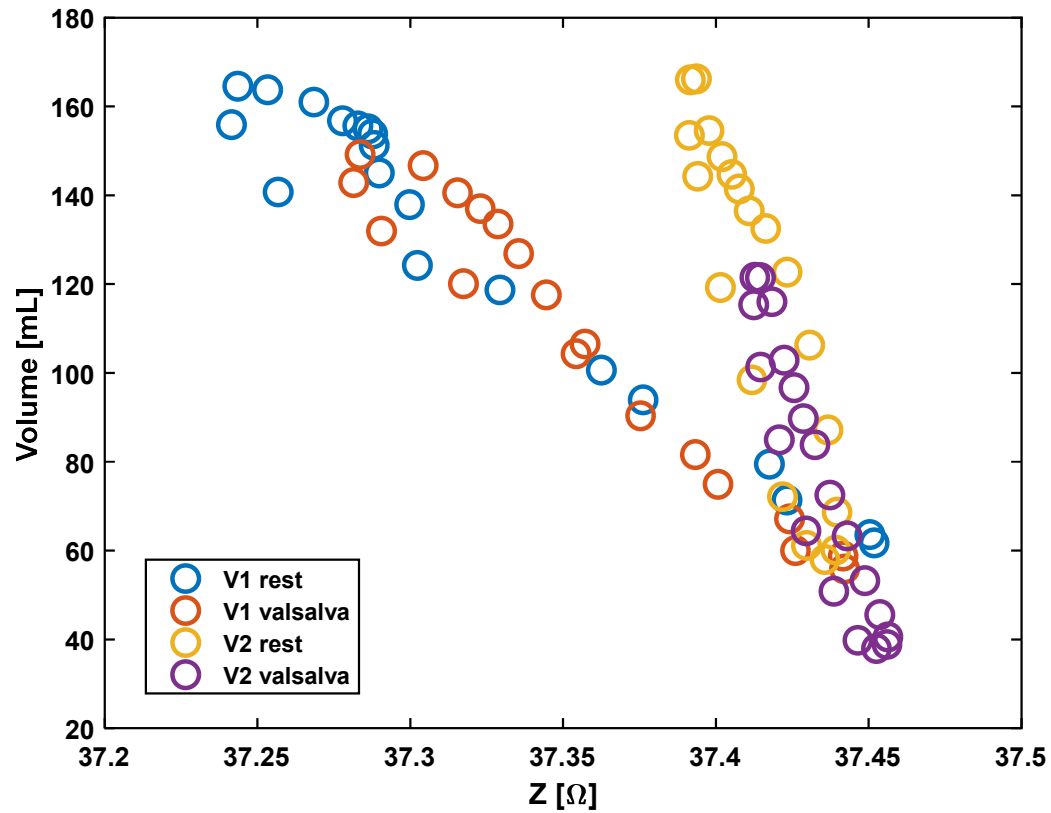
Valsalva manoeuvre changes the stroke volume



Valsalva manoeuvre decreases left ventricular volume



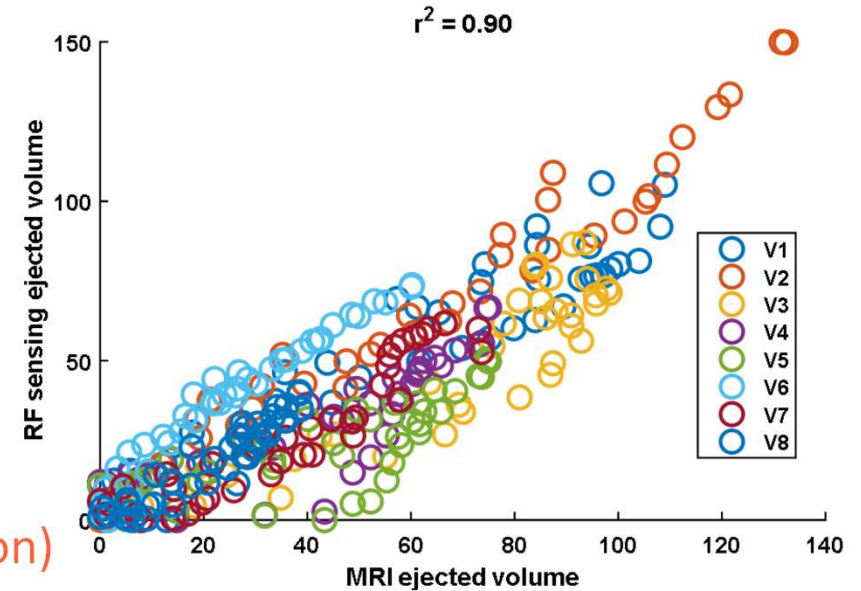
Individual calibration for LV volume is required



Strong correlation observed between RF sensing and MRI measurements



- **Minimize confounding factors**
- E.g. placement
- **However, calibration could be required**
- Subject specific (modelling)
- Population based (modelling + data-driven regression)

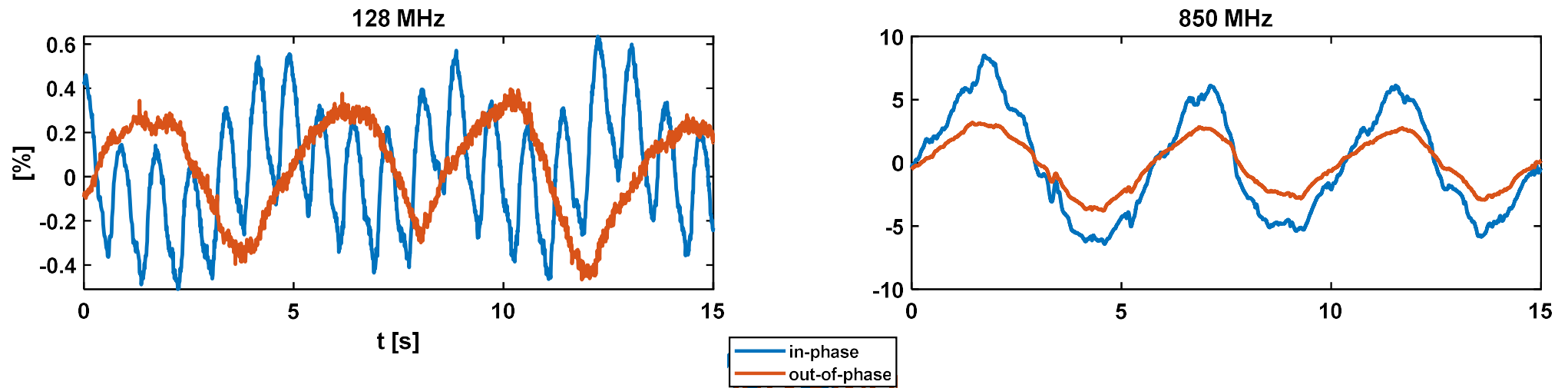


- **Medical imaging, AI and EM simulations important building blocks**



Measurement frequency strongly affects sensitivity to cardiorespiratory motion

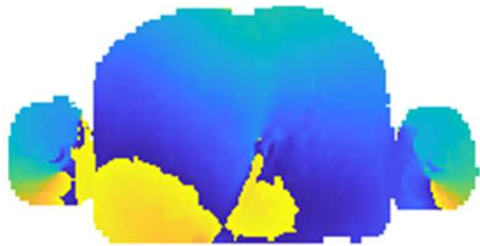
Data acquired on the same subject, in free breathing



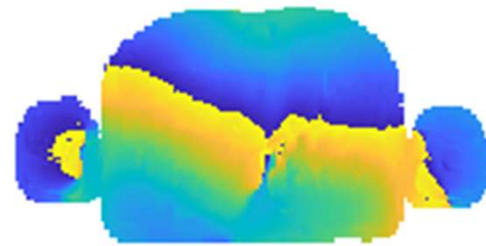
Increasing RF frequency leads to more complex spatial weighing

$$Z_t - Z_0 = -\frac{j\omega}{I^2} \int_V (\epsilon_{r,t} - \epsilon_{r,0}) \overbrace{E_{r,t} \cdot E_{r,0}}^{\text{EM field}} dV$$

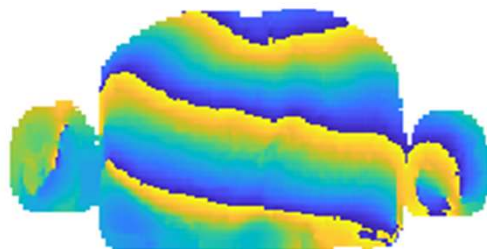
64 MHz



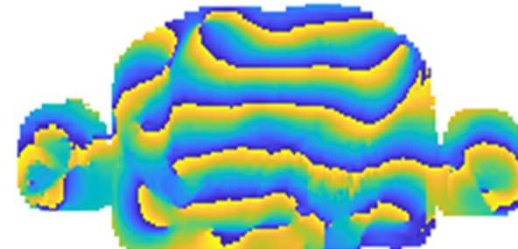
128 MHz



300 MHz



600 MHz

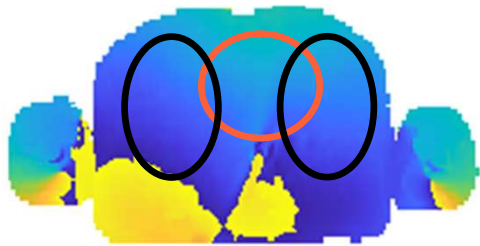


Increasing RF frequency leads to more complex spatial weighing

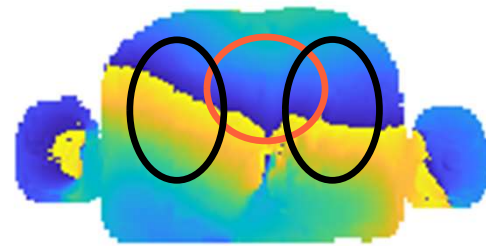
$$Z_t - Z_0 = -\frac{j\omega}{I^2} \int_V (\epsilon_{r,t} - \epsilon_{r,0}) E_{r,t} \cdot E_{r,0} dV$$

- Heart outline
- Lung outline

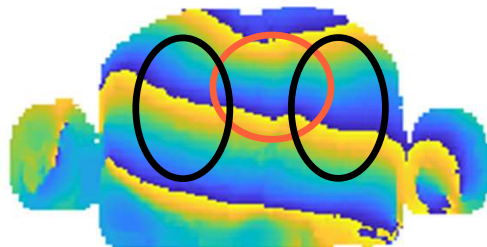
64 MHz



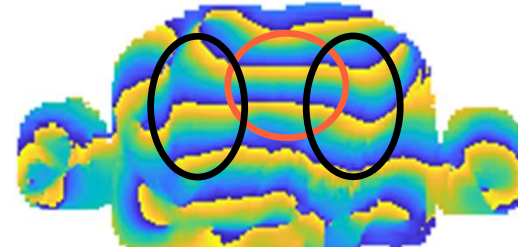
128 MHz



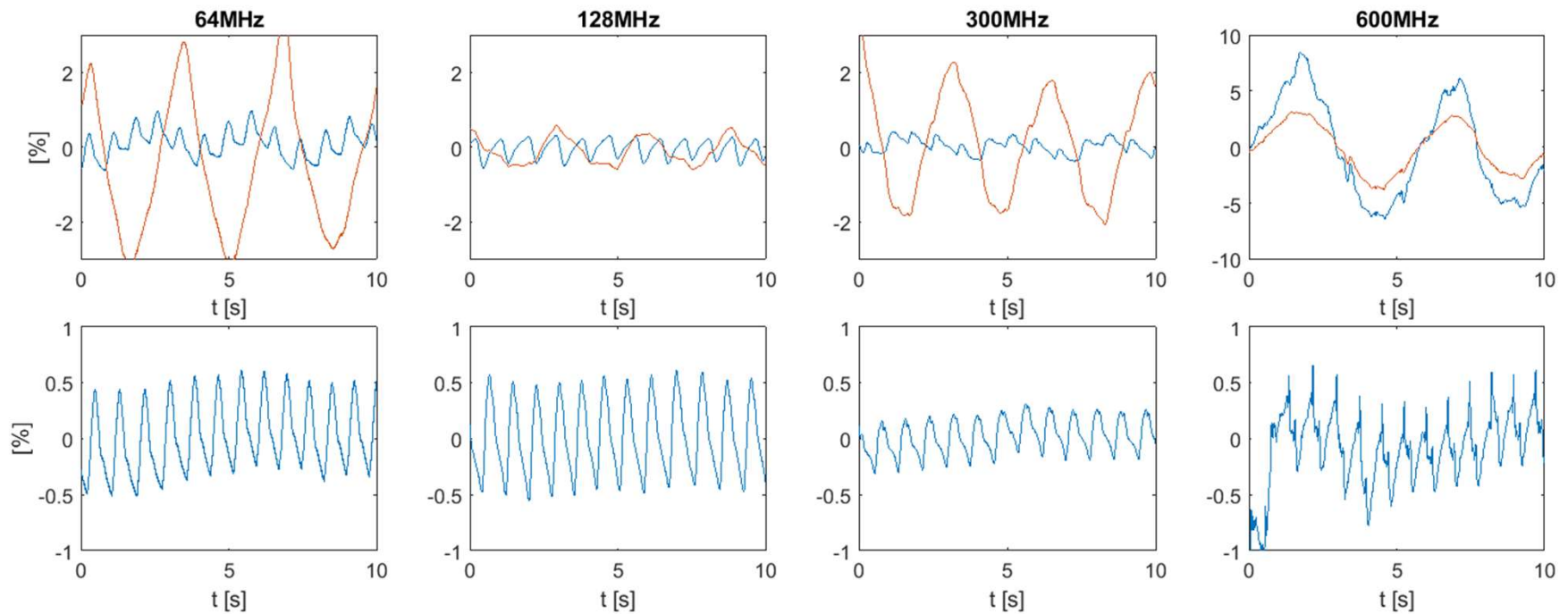
300 MHz



600 MHz

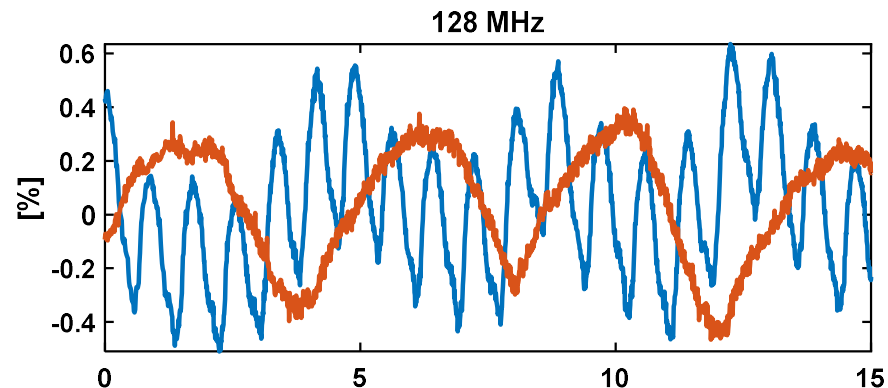


Experimental frequency comparison



Preliminary conclusions on frequency optimization

- At lower frequencies ($< \sim 300$ MHz), better sensitivity to ventricular volume
- Likely sensitive to surface motion or motion of substructures at higher frequencies
 - higher frequencies \rightarrow more spatial encoding capability
- Experimental results best with 128 MHz, best separation between respiratory and cardiac motion



Conclusions and discussion

- Simulation platform enables in-depth study into physical principles and feasibility of RF sensing of stroke volume
- RFS sensing provides none-invasive mechanical information about cardiac function.
- Preliminary validation studies indicate feasibility of measuring stroke volume -> heart failure monitoring
- RF sensing combined with ingredients like MRI, AI and physical modelling will provide new ways of measuring cardio-vascular function outside a hospital setting.

Thank you all

Computational Imaging Group

Nico van den Berg
Alexander Raaijmakers
Christina Louka
Romy O'Connor

Cardiology & Cardiothoracic surgery

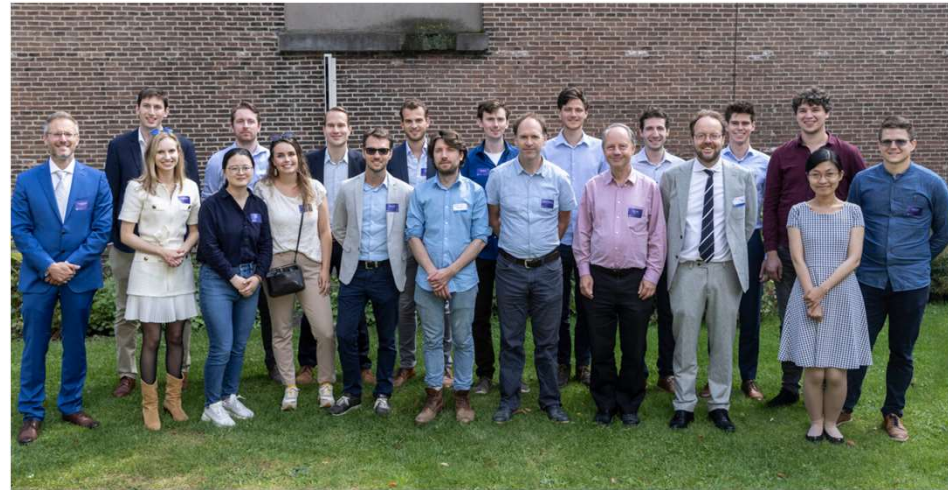
Linda van Laake
Arco Teske
Niels van der Kaaij
Mats Vervoorn

Technology Transfer Office

Frederieke Smeitink
Holger Veenhuis

PrecorDx

Jaap de Bruin



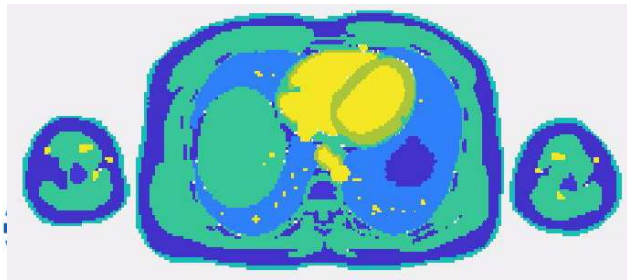
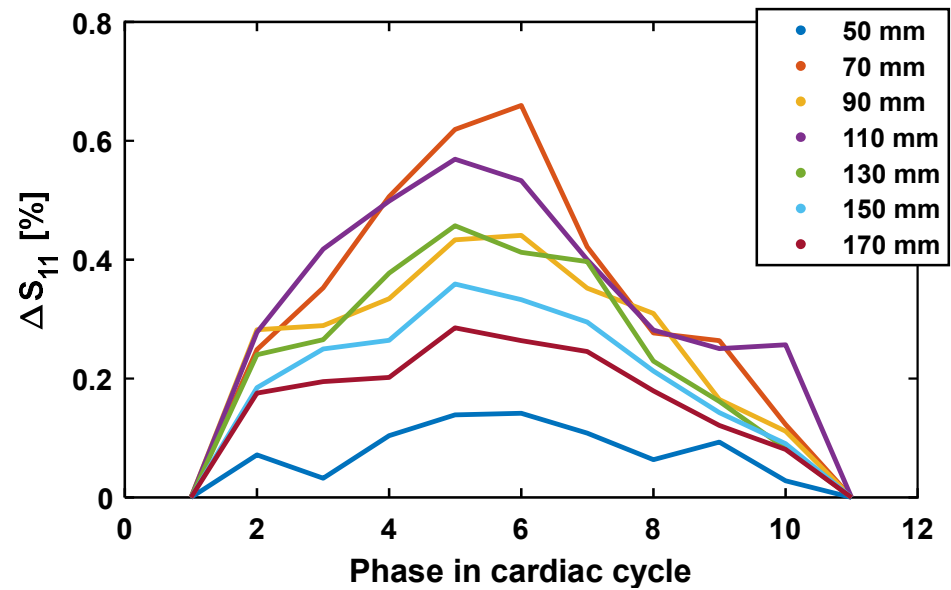
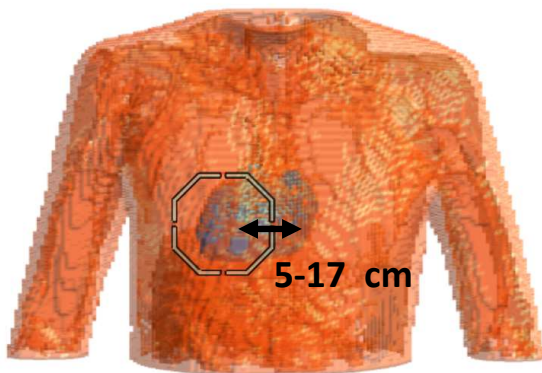
Circulatory Health UMC Utrecht ^{2nd}



Dutch
CardioVascular
Alliance

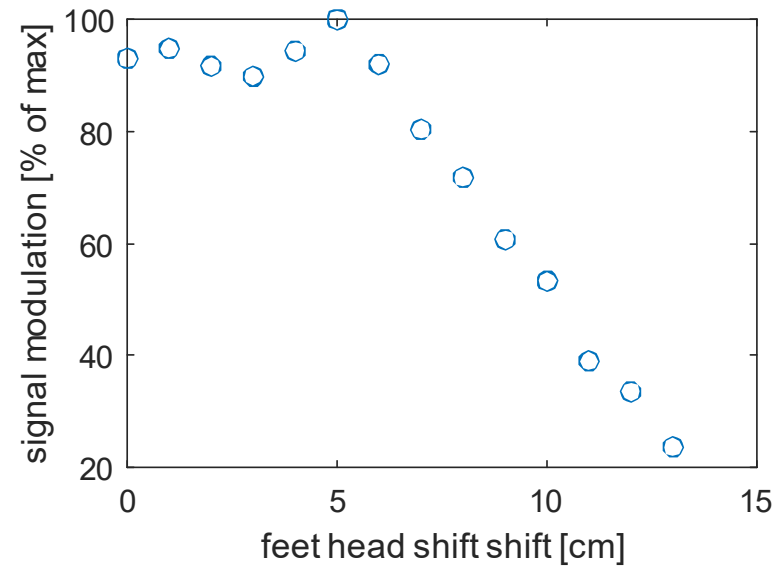
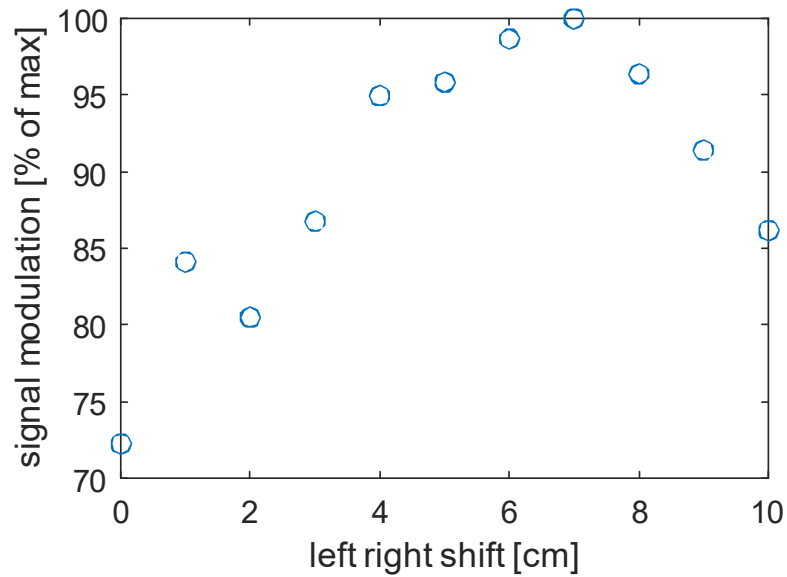
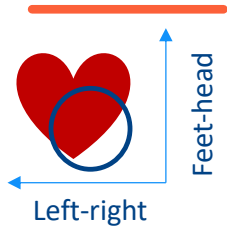
UTRECHT
HOLDINGS

In silico optimization of loop antenna diameter



11 simulations to simulate full cardiac cycle,
11*7 for all different loop sizes

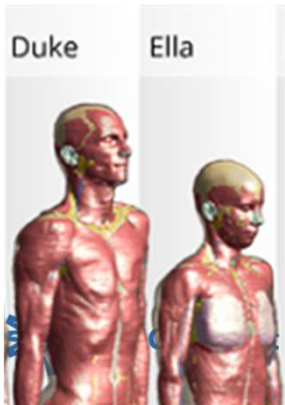
Antenna positioning needs to be precise within ~ 1 cm



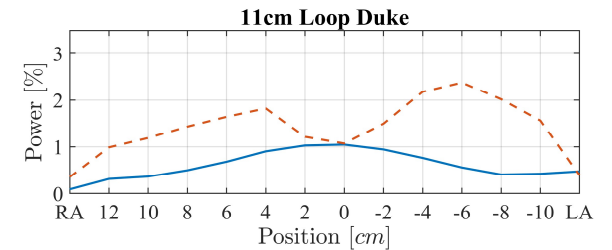
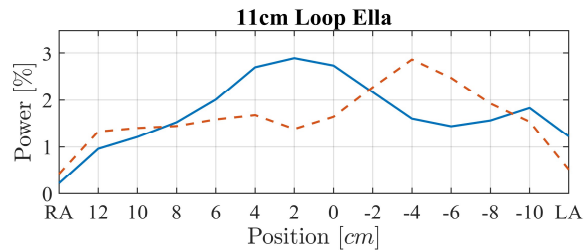
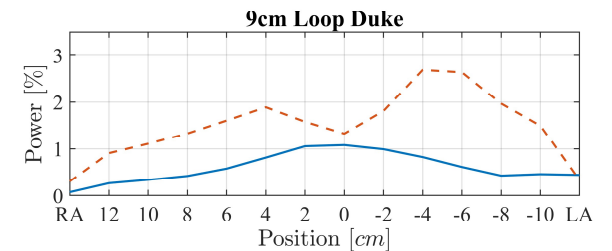
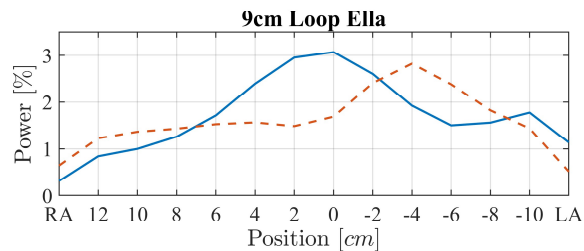
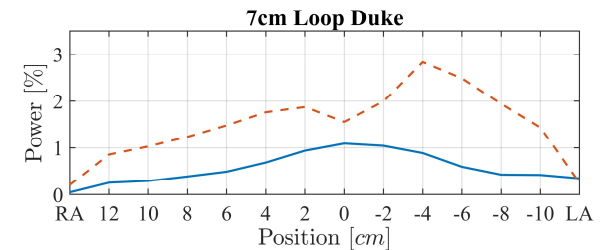
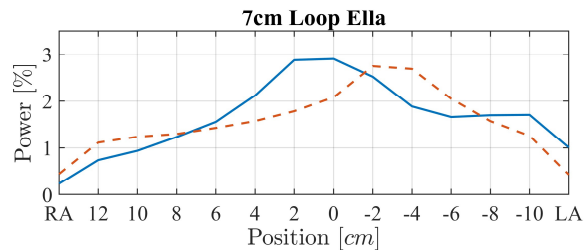
Optimal loop size and position differs per subject



Results from Romy O'Connor



Left & right ventricle power for different loop sizes



— Left Ventricle — Right Ventricle